

Biomaterial Course

Introduction to Biomaterials

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Final Year Bachelor of Chemical Engineering

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BACKGROUND

Historically, biomaterials consisted of materials common in the laboratories of physicians, with little consideration of material properties.

Early biomaterials :

- Gold: Malleable, inert metal (does not oxidize); used in dentistry by Chinese, Aztecs and Romans--dates 2000 years
- Iron, brass: High strength metals; rejoin fractured femur (1775)
- Glass: Hard ceramic; used to replace eye (purely cosmetic)
- Wood: Natural composite; high strength to weight; used for limb prostheses
- and artificial teeth
- Bone: Natural composite; uses: needles, decorative piercings
- Sausage casing: cellulose membrane used for early dialysis (W Kolff)
- Other: Ant pincers. Central American Indians used to suture wounds

Biomaterials are defined by their application, NOT chemical make-up

INTRODUCTION

A biomaterial

- is a nonviable material used in a medical device, intended to interact with biological systems.¹
- is used to make devices to replace a part of a function of the body in a safe, reliable, economic, and physiologically acceptable manner.
- is any substance (other than a drug), natural or synthetic, that treats, augments, or replaces any tissue, organ, and body function.

The need for biomaterials stems from an inability to treat many diseases, injuries and conditions with other therapies or procedures :

- replacement of body part that has lost function (total hip, heart)
- correct abnormalities (spinal rod)
- improve function (pacemaker, stent)
- assist in healing (structural, pharmaceutical effects: sutures, drug release)

¹ Williams, D.F. (1987) Definitions in Biomaterials. Proceedings of a Consensus Conference of the European Society For Biomaterials, England, 1986, Elsevier, New York.

HISTORY

Important dates

- 1860's: Lister develops aseptic surgical technique
- early 1900's: Bone plates used to fix fractures
- 1930's: Introduction of stainless steel, cobalt chromium alloys
- 1938 : first total hip prosthesis (P. Wiles)
- 1940's: Polymers in medicine: PMMA bone repair; cellulose for dialysis; nylon sutures
- 1952: Mechanical heart valve
- 1953: Dacron (polymer fiber) vascular grafts
- 1958: Cemented (PMMA) joint replacement
- 1960: first commercial heart valves
- 1970's: PEO (polyethyleneoxide) protein resistant thin film coating
- 1976: FDA ammendment governing testing & production of biomaterials /devices
- 1976: Artificial heart (W. Kolff, Prof. Emeritus U of U)

MOTIVATION

Improve quality of life...

\$\$\$ Biomaterials is a \$100 billion + market, increasing at 5-7% / yr

- Consider diabetes, which afflicts over 10 million Indians (4% of population)
 - An artificial pancreas, if it existed, and were given to 10% of diabetics would generate over 2.3 billion/yr

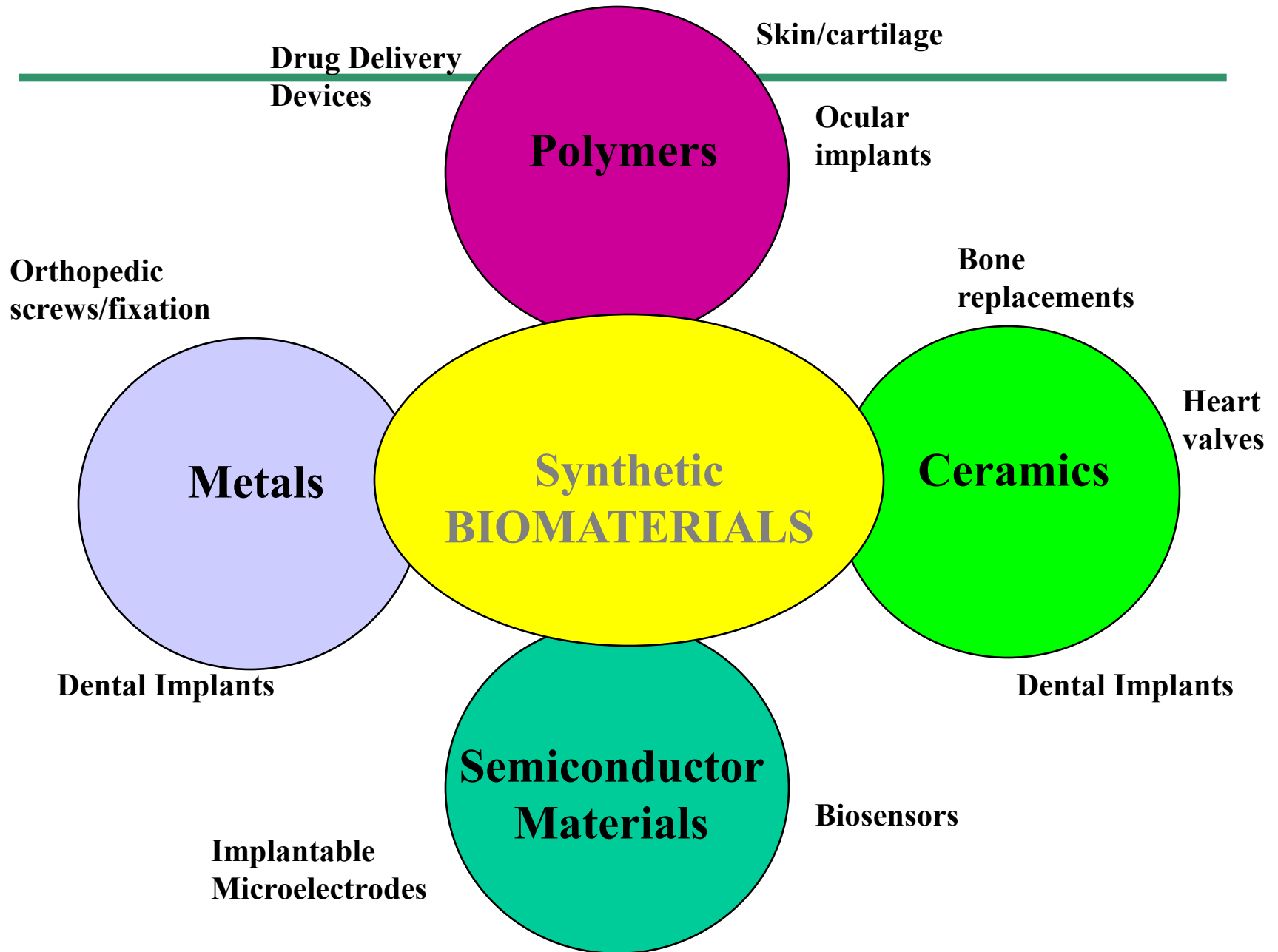
Devices currently on the market²

Device	patient cost	cost of biomaterial	annual revenue (US Data, Indian Data NA)
hemodialyzer	\$18	\$6	\$110M
pacemaker	\$6,000	\$75	\$6.75M
hip	\$3,000	\$100	\$0.5M
stent and catheter	\$3,000	\$30	\$1.75M

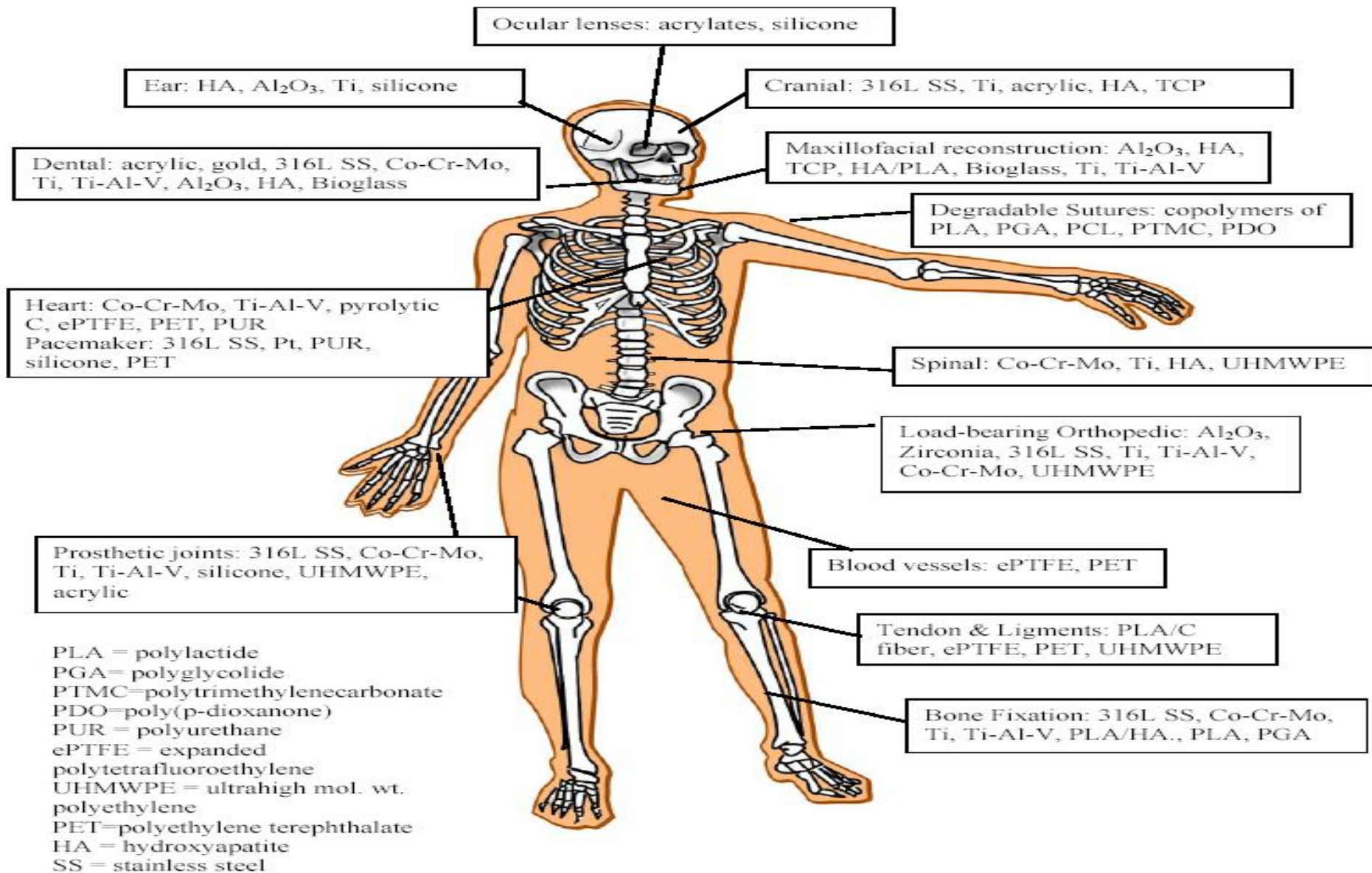
²The Economical Impact of Biomaterials

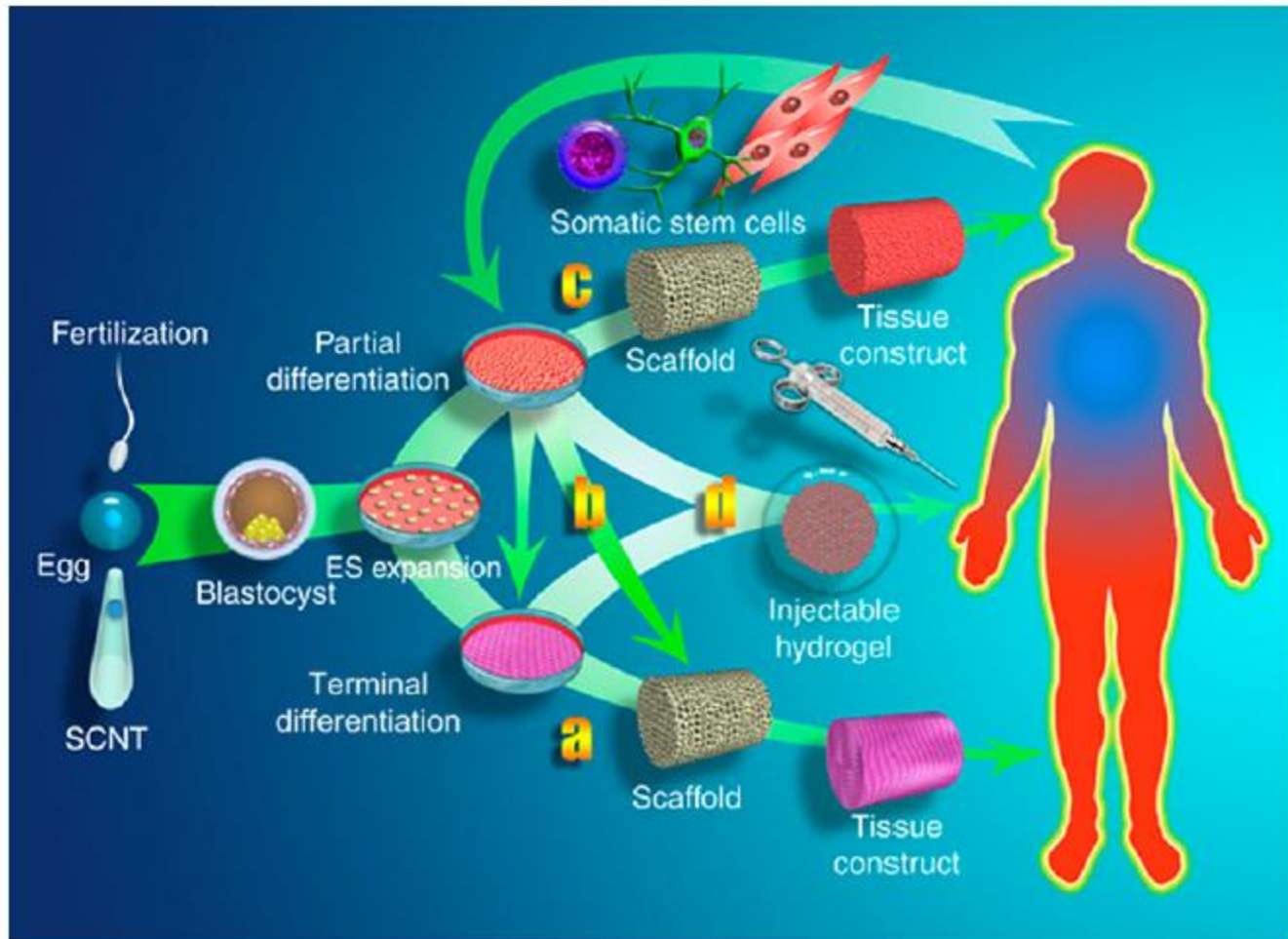
EXAMPLES OF USES OF BIOMATERIALS

Organ/Tissue	Examples
heart	pacemaker, artificial valve, artificial heart
eye	contact lens, intraocular lens
ear	artificial stapes, cochlea implant
bone	bone plate, intramedullary rod, joint prosthesis, bone cement, bone defect repair
kidney	dialysis machine
bladder	catheter and stent
muscle	sutures, muscle stimulator
circulation	artificial blood vessels
skin	burn dressings, artificial skin
endocrine	encapsulated pancreatic islet cells

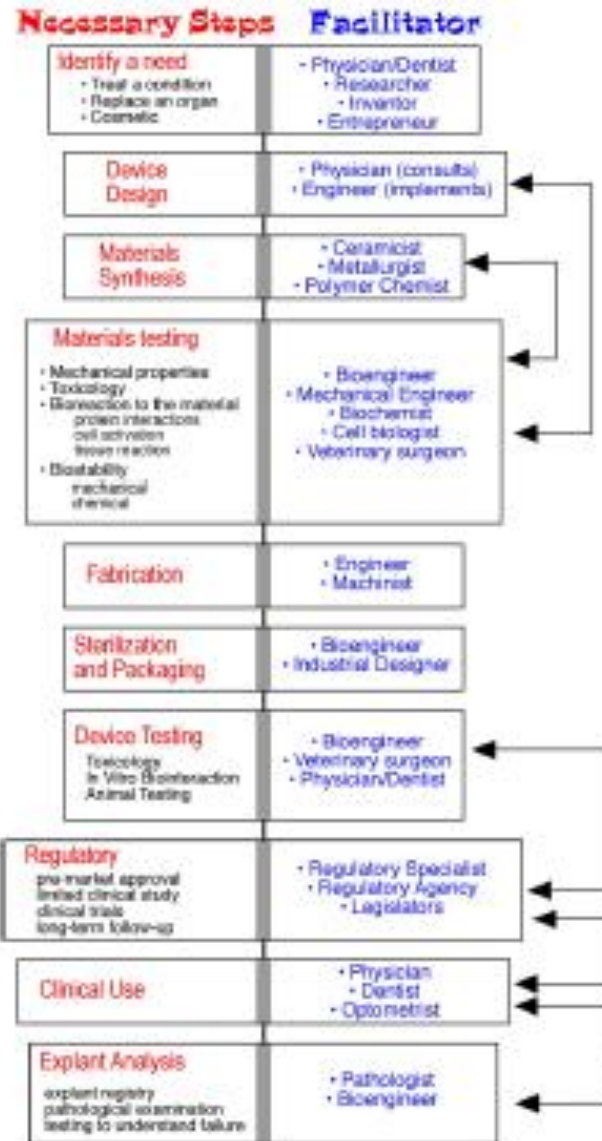


Biomaterial Science





Need



MATERIAL ATTRIBUTES FOR BIOMEDICAL APPLICATIONS

Property	Desirables
Biocompatibility	Noncarcinogenic, nonpyrogenic, nontoxic, nonallergenic, blood compatible, non-inflammatory
Sterilizability	Not destroyed by typical sterilizing techniques such as autoclaving, dry heat, radiation, ethylene oxide
Physical characteristics	Strength, elasticity, durability
Manufacturability	Machinable, moldable, extrudable

BIOCOMPATIBILITY

There is no general set of criteria, that if met, qualify a material as being biocompatible

- The time scale over which the host is exposed to the material or device must be considered

material	contact time
syringe needle	1-2 s
tongue depressor	10 s
contact lens	12 hr - 30 days
bone screw / plate	3-12 months
total hip replacement	10-15 yrs
intraocular lens	30 + yrs

“Biocompatibility” is strongly determined by primary chemical structure !

Classes of Biomaterials

- Metals
 - stainless steel, cobalt alloys, titanium alloys
- Ceramics
 - aluminum oxide, zirconia, calcium phosphates
- Polymers
 - silicones, poly(ethylene), poly(vinyl chloride), polyurethanes, polylactides
- Natural polymers
 - collagen, gelatin, elastin, silk, polysaccharides

Material Properties

OBJECTIVES

To introduce the fundamental mechanical and surface chemistry properties of biomaterials

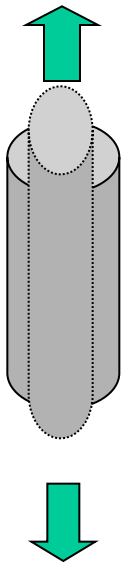
OUTLINE

- Mechanical Properties
 - elasticity, viscoelasticity, brittle fracture, fatigue
- Surface chemistry

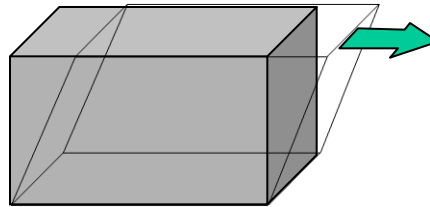
Mechanical Properties

Many applications require the biomaterial to assume some of the applied **load** on the body part.

tension



shear



Viscoelasticity

The response of materials to an imposed stress may under certain conditions resemble the behavior of a solid or a liquid.

Stress Relaxation (application of a sudden strain to the sample and following the stress as a function of time as the strain is held constant).

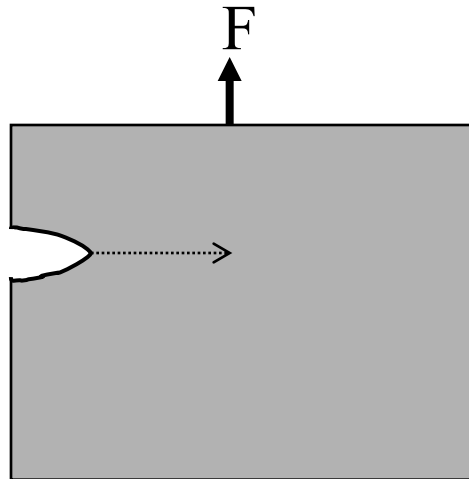
Creep (a constant stress is instantaneously applied to the material and the resulting strain is followed as a function of time)

Creep is function of crystallinity: As % crystallinity increases, creep decreases

Brittle Fracture

Calculated ultimate tensile strengths are large compared to measured ultimate tensile strengths.

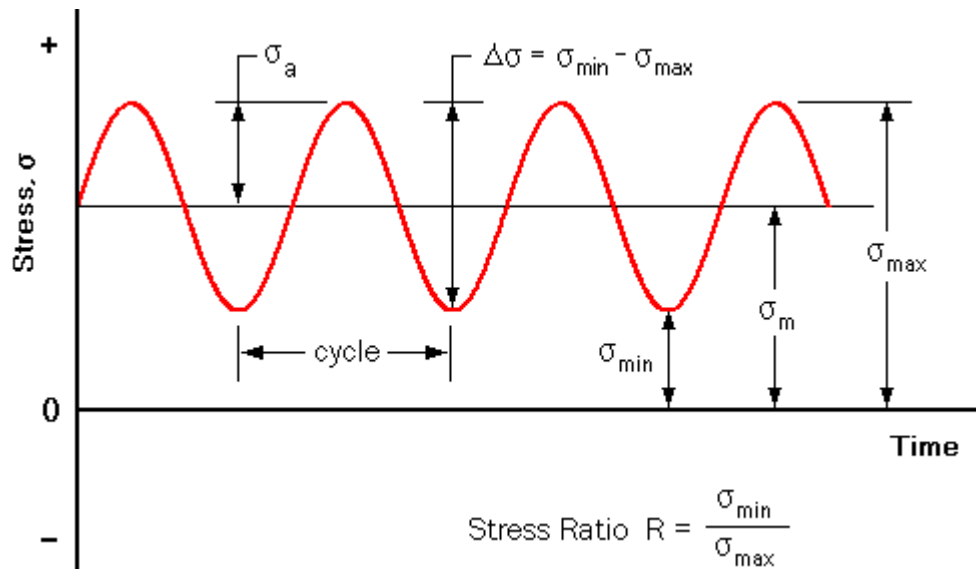
$$K_{Ic} = Y\sigma_f\sqrt{\pi C}$$



Fatigue

The progressive deterioration of the strength of a material or structural component during service such that failure can occur at much lower stress levels than the ultimate stress of the material.

Cyclic Fatigue



Surface Energy

Interface

- boundary between 2 layers

significance

- protein adsorption to materials
- blood coagulation/thrombosis due to material contact
- cellular response to materials

Surface Chemistry

Primary

- Ionic: e^- donor, e^- acceptor *ceramics, glasses (inorganic)*
- Covalent: e^- sharing *glasses, polymers*
- Metallic: e^- “gas” around lattice of + nuclei

Secondary/Intermolecular

- Electrostatic
- H-bonding
- Van der Waals (dipole-dipole, dipole-induced dipole, London dispersion)
- Hydrophobic Interactions (entropy-driven clustering of nonpolar gps in H_2O)
- Physical Entanglement (high MW polymers)

Ex. 1: alumina Al_2O_3
(corundum)

used for hard tissue replacement –
e.g., dental implants

Properties:

- corrosion resistant
- high strength
- wear resistant
- “biocompatible”

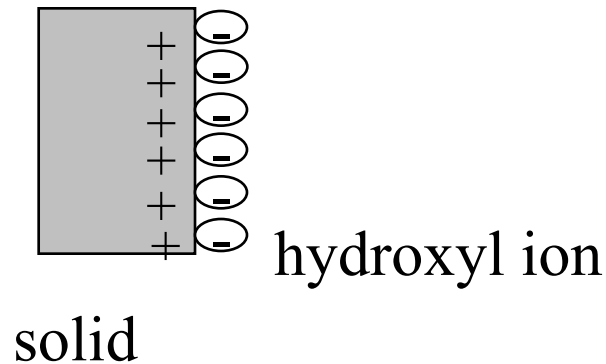
derived from
ionic bonding

Electrostatic interactions w/ charges on
proteins \Rightarrow non-denatured adsorbed protein
layer \Rightarrow “camouflage”

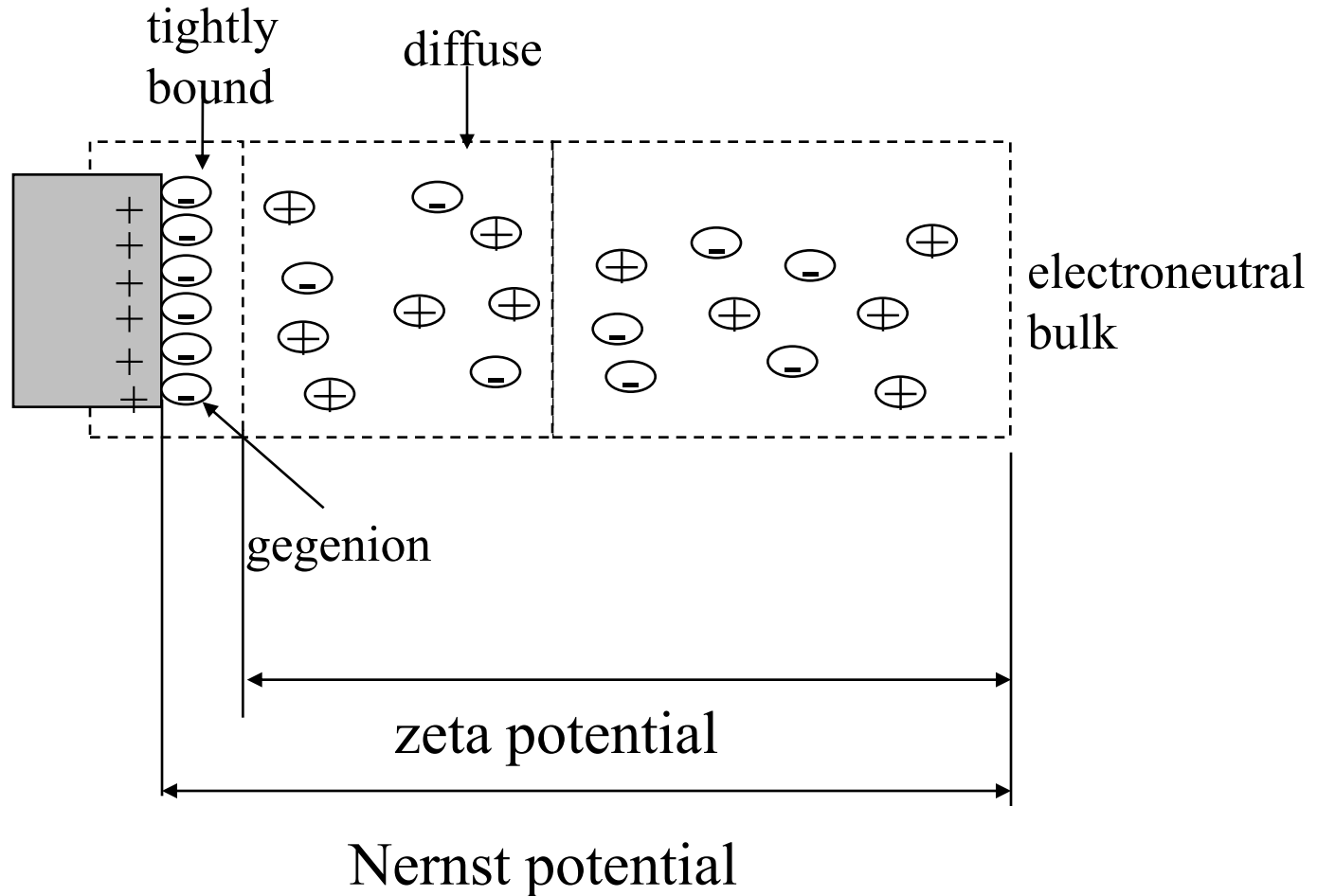
Surface Electrical Properties

surface may become charged by

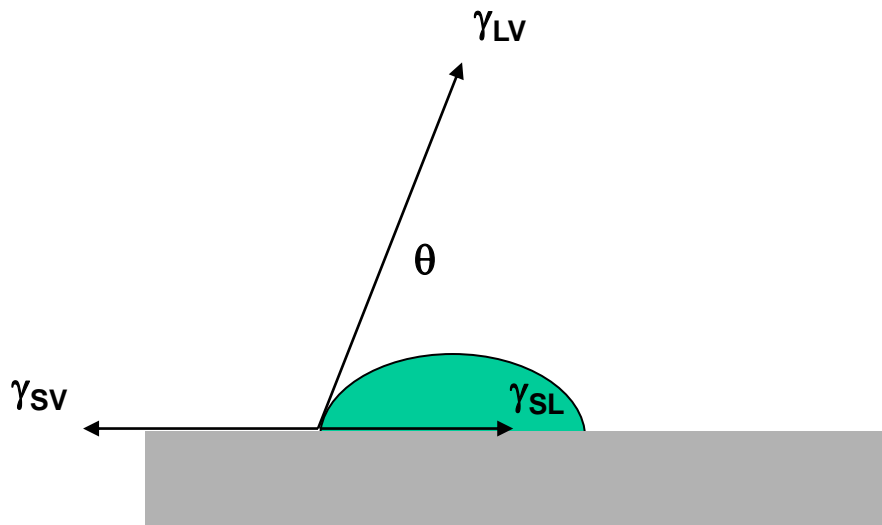
- adsorption of ionic species present in sol'n or preferential adsorption of OH^-
- ionization of $-\text{COOH}$ or $-\text{NH}_2$ group



Electric Double Layer



Surface Energy and the Contact Angle



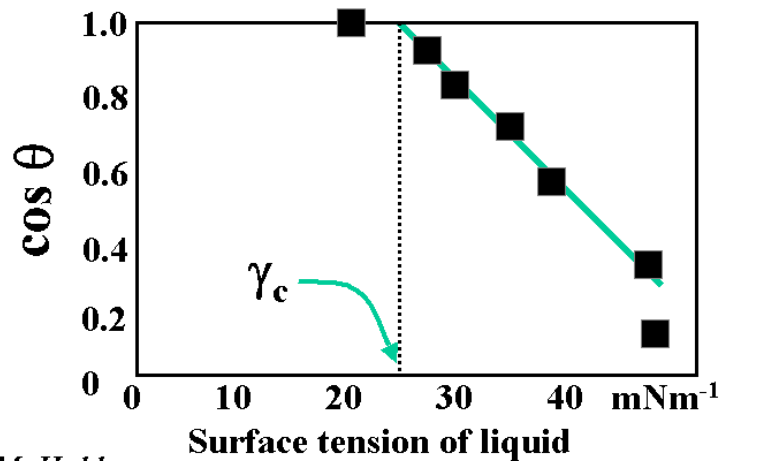
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Critical Surface Tension, γ_c

The critical surface tension is the surface tension of a liquid that would completely wet the solid of interest.

Zisman plot to determine γ_c



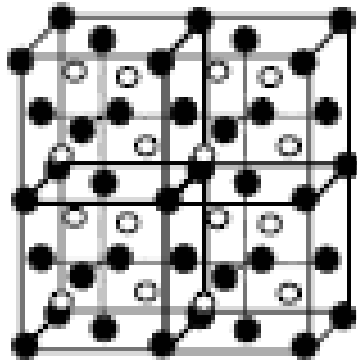
M. Hubbe

Schematic

Material	γ_c (dyne/cm)
Co-Cr-Mo	22.3
Pyrex glass	170
Gold	57.4
poly(ethylene)	31-33
poly(methylmethacrylate)	39
Teflon	18

Higher Order Structures

Crystals: 3D periodic arrays of atoms or molecules



*metals, ceramics,
polymers (semicrystalline)*

crystallinity decreases solubility and bioerosion
(biodegradable polymers & bioresorbable ceramics)

Networks: exhibit short range order & characteristic lengths

inorganic glasses, gels

Ex. 1: Bioactive Glasses

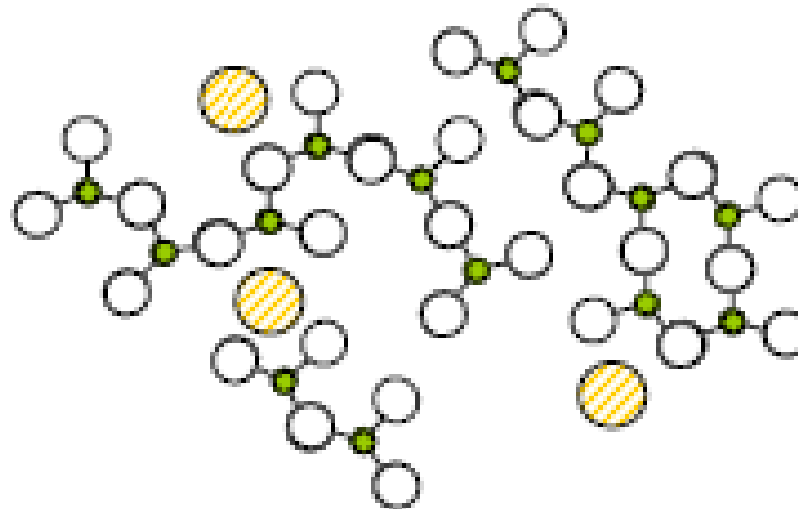
used for hard connective tissue replacement

Network formers (~50wt%): SiO_2 , P_2O_5

Network modifiers (high! ~50wt%): Na_2O , CaO

Properties:

- partially soluble *in vivo* (facilitates bone bonding)
 - easily processed (complex shapes)
- } derived from loose ionic network



Other Ex. Hydrogel, Self assemblies, micelles, liposomes

Microstructures

Ex. 1: Porous Bioresorbable Scaffolds polylactide (PLA)

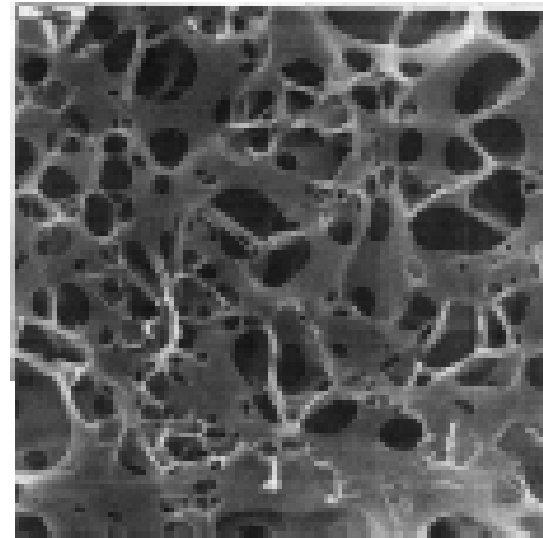
used for tissue
regeneration

Properties:

- Penetrable to body fluids, cells
- Structurally stable

derived from pore
microstructure

Pore dimensions:
10-100 μm



Other: crystal grain, spherulites etc.

Thank You